



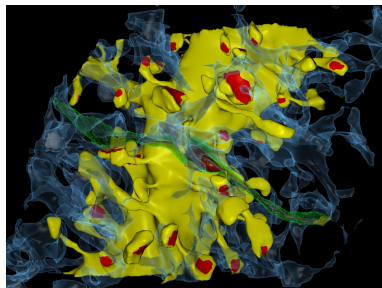
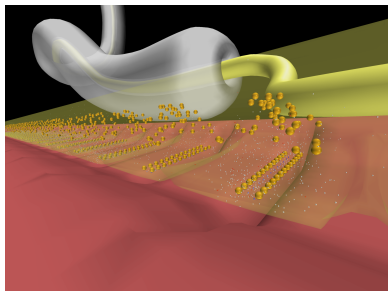
Overview of MCell Methods

Markus Dittrich
dittrich@psc.edu

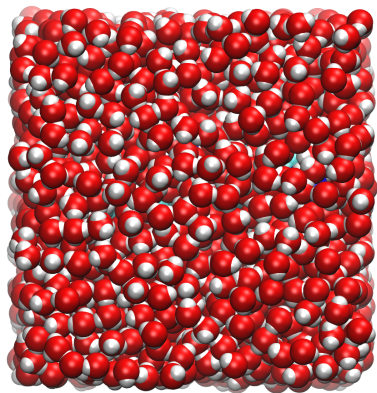
National Center for Multiscale Modeling of Biological Systems (MMBioS)
Biomedical Applications Group, Pittsburgh Supercomputing Center, CMU

April 27, 2014

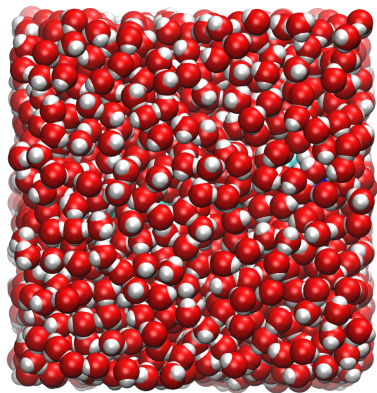
- 1 Computational Microphysiology
- 2 Biomolecular Systems at the Molecular Level
- 3 Biomolecular Systems at the Microphysiological Level
- 4 Diffusion Theory
- 5 Monte Carlo Probabilities For Diffusion in MCell
- 6 Monte Carlo Probabilities For Unimolecular Transitions in MCell
- 7 Monte Carlo Probabilities For Bimolecular Associations in MCell
- 8 Monte Carlo Probabilities For Volume Reactions in MCell
- 9 References



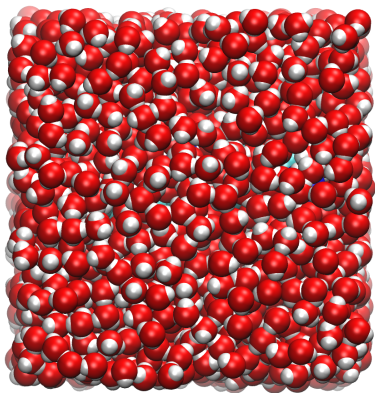
We want to simulate realistic 3D cellular microphysiology at length scales from nm and up and timescales of ns and longer.



- To a first approximation, at the molecular level cells mostly consist of biomolecules solvated by (a large number of) water molecules.

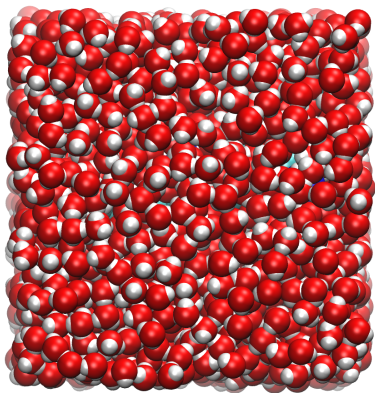


- To a first approximation, at the molecular level cells mostly consist of biomolecules solvated by (a large number of) water molecules.
- Relevant time and length scales are fs ($10^{-15}s$) and \AA ($10^{-10}m$).

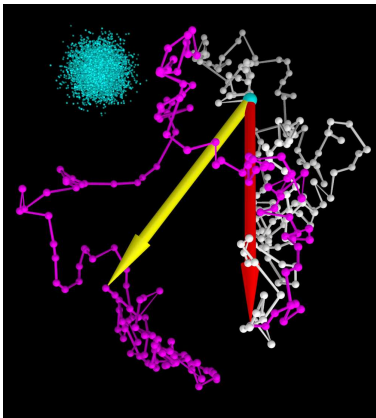


- To a first approximation, at the molecular level cells mostly consist of biomolecules solvated by (a large number of) water molecules.
- Relevant time and length scales are fs ($10^{-15}s$) and \AA ($10^{-10}m$).
- At room temperature ($25^\circ C$) water molecules move rapidly. From equilibrium statistical mechanics

$$\bar{v} = \sqrt{\frac{3kT}{m}} = 640 \text{ m/s}$$



- To a first approximation, at the molecular level cells mostly consist of biomolecules solvated by (a large number of) water molecules.
- Relevant time and length scales are fs ($10^{-15}s$) and \AA ($10^{-10}m$).
- At room temperature ($25^\circ C$) water molecules move rapidly. From equilibrium statistical mechanics
$$\bar{v} = \sqrt{\frac{3kT}{m}} = 640 \text{ m/s}$$
- Frequent collisions of solute with water molecules randomizes their movement. Molecular motions are highly correlated.



- At the microphysiological level we are concerned with biology at time and length scales on the order of μs ($10^{-6}s$) or longer and μm ($10^{-6}m$) and up.
- At these scales molecular motion becomes uncorrelated and we can, to a first approximation, ignore water molecules and their rapid motion and instead describe molecular movement by stochastic *Brownian Motion* combined with a *diffusion coefficient*.
- Algorithms for simulations at the cellular level are typically based on PDE/finite element or stochastic methods.

Developed by physiologist Adolf Fick in 1855.

Fick's 1st Law:

$$\mathbf{J}(\mathbf{r}, t) = -D(C, t) \nabla C(\mathbf{r}, t) \quad (1)$$

Fick's 2nd Law:

$$\frac{\partial C(\mathbf{r}, t)}{\partial t} = \nabla (D(C, t) \nabla C(\mathbf{r}, t)) = D(C, t) \nabla^2 C(\mathbf{r}, t) \quad (2)$$

Eq. 2 is called the **Diffusion Equation**.

Here, J , diffusion flux [$\text{Mol length}^{-2} \text{ time}^{-1}$], D , diffusion coefficient [$\text{length}^2 \text{ time}^{-1}$, $\text{cm}^2 \text{ s}^{-1}$], C concentration [Mol length^{-3} , mol l^{-1}].

The solution to Fick's 2nd Law provides the basis for MCell diffusion algorithm.

$$\frac{\partial C(\mathbf{r}, t)}{\partial t} = D(C, t) \nabla^2 C(\mathbf{r}, t) \quad (3)$$

In the neighborhood of a given molecule location, the concentration C can be assumed to be radially symmetric, $C(\mathbf{r}, t) \equiv C(r, t)$ and Eq. 3 simplifies to

$$\frac{\partial C(r, t)}{\partial t} = D(C, t) \frac{\partial^2 C(r, t)}{\partial^2 r} \quad (4)$$

Equation can be solved analytically for certain boundary conditions. E.g. for a point source of M molecules the solution becomes

$$C(r, t) = \frac{M}{\lambda^3 \pi^{3/2}} e^{-r^2/\lambda^2}, \quad \lambda = \sqrt{4Dt} \quad (5)$$

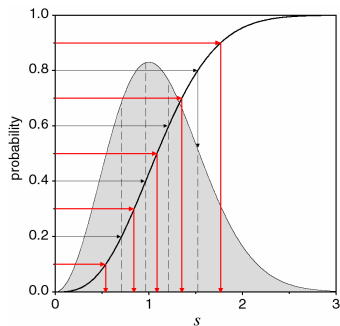
Eq. 5 can be directly converted into the fractional probability p_r for a displacement between r and $(r + dr)$ for a single diffusing molecule:

$$p_r = \frac{1}{\lambda^3 \pi^{3/2}} e^{-r^2/\lambda^2} (4\pi r^2) dr \quad (6)$$

$$p_s = \frac{4}{\sqrt{\pi}} s^2 e^{-s^2} ds \quad , \quad s = \frac{r}{\lambda} = \frac{r}{\sqrt{4Dt}} \quad (7)$$

Using Eq. 6 we can also compute the mean radial displacement \bar{l}_r

$$\bar{l}_r = \frac{2}{\pi} \lambda \sim \sqrt{t} \quad (\bar{l}_\perp = \frac{\bar{l}_r}{2}) \quad (8)$$



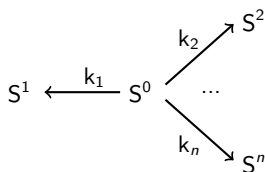
$$p_s = \frac{4}{\sqrt{\pi}} s^2 e^{-s^2} ds$$

$$s = \frac{r}{\sqrt{4Dt}}$$

To choose a radial distance R for diffusion we pick a random number X in $[0, 1]$ and solve

$$X = CDF(R) = \int_0^R p_s ds = \text{erf}(R) - \frac{2}{\sqrt{\pi}} R e^{-R^2} \quad (9)$$

This can be efficiently computed during runtime of the simulation.



Unimolecular transition: Initial state S^0 can undergo one of n possible transitions to states S^1 through S^n with first order rate constants k_1, k_2, \dots, k_n .

We need to know the probability p_t that a single molecule in S^0 undergoes a transition. p_t is given by the fraction of $[S^0]$ that undergoes a transition during time t :

$$p_t = \frac{[S^1]_t + [S^2]_t + \dots + [S^n]_t}{[S^0]_0} = 1 - \frac{[S^0]_t}{[S^0]_0} \quad (10)$$

From the rate equation we obtain

$$-d[S^0] = (k_1 + k_2 + \dots + k_n)[S^0]dt = \left(\sum_{j=1}^n k_j \right) [S^0]dt \quad (11)$$

Eq. 11 can be integrated

$$\int_{[S^0]_0}^{[S^0]_t} \frac{d[S^0]}{[S^0]} = - \left(\sum_{j=1}^n k_j \right) \int_0^t dt \quad (12)$$

to yield

$$\frac{[S_0]_t}{[S_0]_0} = e^{-\sum_{j=1}^n k_j t} \quad (13)$$

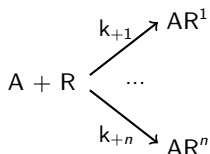
Substituting Eq. 13 into Eq. 10 then gives the probability p_t for unimolecular transitions as (here τ is the mean lifetime of S^0)

$$p_t = 1 - e^{-\sum_j k_j t}, \quad \tau = 1 / \sum k_j \quad (14)$$

$$p_1 = p_t \frac{k_1}{\sum_j k_j}, \quad \dots \quad p_n = p_t \frac{k_n}{\sum_j k_j}; \quad \sum_i p_i = p_t \quad (15)$$

Notes:

- The naïve way to choose unimolecular reactions is to compare a single random number in $[0, 1]$ to the cumulative probabilities $(p_{k1}, p_{k1} + p_{k2}, \dots, 1)$.
- MCell3 instead computes the lifetime of each molecule from the exponential distribution of lifetimes $\rho(t) = \frac{1}{\tau} e^{-t/\tau}$ and then uses its *scheduler* to schedule the unimolecular reaction to occur at the appropriate time.



Bimolecular Association: An example would be association between ligand A (volume molecule) and receptor R (surface molecule) with n possible binding sites.

We will derive a relation for p_b , the binding probability of ligand A to receptor R. The average rate of binding p_{bt} after N_H hits is given by

$$p_{bt} = 1 - (1 - p_b)^{N_H} \quad (16)$$

Next, we require that the *average binding rate* is equal to binding rate predicted by *mass action kinetics* given by

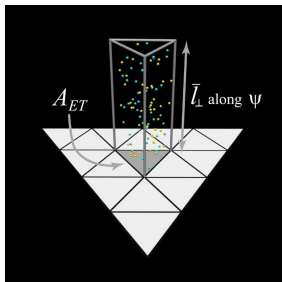
$$p_t = \sum_i k_{+i} [A]_0 \Delta t \quad , \quad \Delta t \rightarrow 0 \quad (17)$$

$$1 - (1 - p_b)^{N_h} = p_{bt} = p_t = \sum_i k_{+i} [A]_0 \Delta t \quad (18)$$

For small Δt , p_b and N_H approach zero and thus $(1 - p_b)^{N_H} \approx (1 - N_H p_b)$. Thus, Eq. 18 simplifies to

$$p_b = \sum_i k_{+i} \frac{[A]_0 \Delta t}{N_H}, \quad \Delta t \rightarrow 0 \quad (19)$$

Next, we need to derive a relation for N_H the number of hits of A on R



The number of hits per unit time on a tile with surface area A_{ET} is given by

$$hits = 0.5 N_a \frac{\bar{l}_{\perp}}{\Delta t} A_{ET} [A]_0 \quad (20)$$

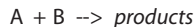
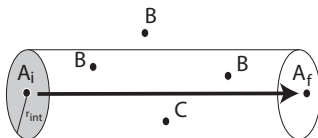
This results in ($\Delta t \rightarrow 0$)

$$N_H = \int_0^{\Delta t} hits dt \approx N_a A_{ET} [A]_0 \left(\frac{4D}{\pi} \right)^{1/2} \Delta t \quad (21)$$

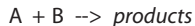
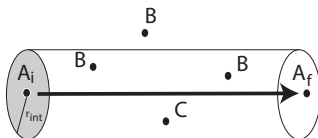
Eliminating N_H in Eq. 19 with 21 then yields the final expression for p_b

$$p_b = \sum_i k_{+i} \frac{1}{2N_a A_{ET}} \left(\frac{\pi \Delta t}{D} \right)^{1/2} \quad (22)$$

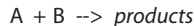
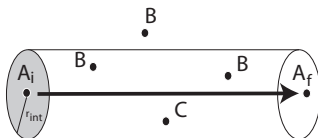
This can be efficiently computed at system initialization.



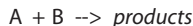
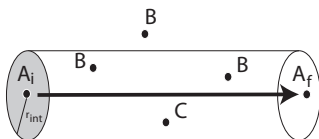
- Volume molecules in MCell diffuse via ray-tracing along a randomly selected direction and diffusion step length computed as explained previously.



- Volume molecules in MCell diffuse via ray-tracing along a randomly selected direction and diffusion step length computed as explained previously.
- Reaction partners are discovered and tested for reactions during ray marching. This unique approach provides good correlation between diffusive motion and location of reactants.



- Volume molecules in MCell diffuse via ray-tracing along a randomly selected direction and diffusion step length computed as explained previously.
- Reaction partners are discovered and tested for reactions during ray marching. This unique approach provides good correlation between diffusive motion and location of reactants.
- For the purpose of collision detection reactants acquire an interaction radius.



- Volume molecules in MCell diffuse via ray-tracing along a randomly selected direction and diffusion step length computed as explained previously.
- Reaction partners are discovered and tested for reactions during ray marching. This unique approach provides good correlation between diffusive motion and location of reactants.
- For the purpose of collision detection reactants acquire an interaction radius.

Using an argument analogous to the one for bimolecular associations we can derive the following relation for the reaction probability between two diffusing volume molecules with diffusion constants D_1 and D_2 :

$$p = \frac{k}{4A_{int}} \left(\frac{\pi \Delta t}{D_1 + D_2} \right)^{1/2} \quad (23)$$

Stiles, JR, and Bartol, TM. (2001). *Monte Carlo methods for simulating realistic synaptic microphysiology using MCell*. In: Computational Neuroscience: Realistic Modeling for Experimentalists, ed. De Schutter, E. CRC Press, Boca Raton, pp. 87-127.

Kerr R, Bartol TM, Kaminsky B, Dittrich M, Chang JCJ, Baden S, Sejnowski TJ, Stiles JR. (2008). *Fast Monte Carlo Simulation Methods for Biological Reaction-Diffusion Systems in Solution and on Surfaces*. SIAM J. Sci. Comput., 30(6):3126-3149.